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**ABSTRACT** 

a. REPORT | b. ABSTRACT | c. THIS PAGE

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# Building and Validating a Model of Human Blast Traumatic Brain Injury: A Hybrid Computational and Experimental Approach

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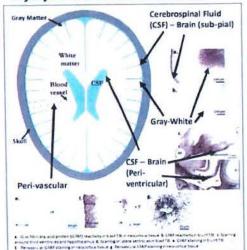
Introduction

Nearly 150,000 of the returning soldiers from Iraq and Afghanistan have suffered blast induced Traumatic Brain Injury (TBI), leaving the victims at risk for persistent neurologic/behavioral symptomatology, including headaches, sleep disorder, cognitive impairment and mood disturbance. Although defining what the mury of blast TBI is has been difficult and prone to confounders, looking to clinical data has helped differentiate this injury from other TBI in theater experience from the physicians who treated blast victims identified some unique features of this injury, injury to the blood vessels at both large and small length scales manifesting with brain swelling, subarachnold hemorrhage or pseudoaneurysm and vasospasm [1-4]. More recently, careful neuropathologic studies of victims of blast TBI demonstrated a unique pattern of astroglial scaring at multiple intracranial interfaces subplat, perivascular, periventricular, and gray white junction [5]. However, the mechanism(s) and threshold of these injuries have not been resolved mechanically, thus protective equipment cannot be optimized to reduce the injury. The purpose of this work is build a model which reproduces the human intracranial injury after blast exposure in order to isolate the mechanism(s) of injury

### Hypotheses

Observed patterns of blast traumatic brain injury can be explained by the focusing of blast stress waves that occur at the intracranial mechanical interfaces (CSF brain, vessel brain, gray white, etc)

## Pathology of Blast Traumatic Brain Injury at Mechanical Interfaces [5]



### Mechanical Properties of Cranial Contents [6]

	Destring	Bulk Modelus	Shear Modules
Skull	1.21 (g/cc)	4672 (MPa)	3270 MPa
White Matter	1.04	2371	41 kPa-Go. 7.8 kPa-God 8 = 40 * 2
Gray Matter	1.04	2371	34 kPa-G <sub>a</sub> , 6.4 kPa-G <sub>art</sub> B = 40 *1
CSF	.9998	1960	

### **Computational Methods**

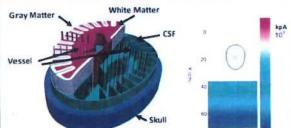
The material models utilized in CTH and Sierra are fit to material property data of human tissue published in the open iterature for bone, white matter, gray matter, and cerebrospinal fluid. These material mode's have been previously employed and validated in modeling & simulation of blast and blunt impact of human models by Taylor et al. of Sandia National Laboratories (6-9)

#### Computational integration - Eulerian (CTH)

CTM is an fulerian finite volume computer simulation code that is capable of tracking 90+ materials simultaneously, simulating their interactions as they undergo blast loading. This code is is a validated shock physics simulation suite and has been used to study fluid-solid interactions that occur between blast waves and the test object model [10]. Blast wave was modeled as a slab of energized with overpressure of J60kPa

#### Computational integration - Immersed Lagrangian (Sierra)

Sierra mechanics is the finite element simulation suite developed by Sandra National labs to predict behavior of complex structures under extreme loading Biast loading is accomplished by passing pressures from CTH to Sierra/SM, where they are used as a boundary condition for the finite element simulation. This one way coupling is sufficient for large over pressure loadings. Future work will utilize a two way coupling for lower amplitude blast studies

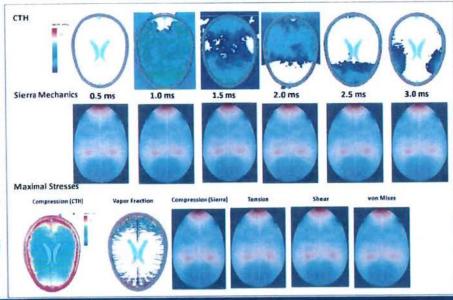


#### Computational Test Object

kpA The test object employed within CTH is comprised of 5 explicit materials with a spatial resolution of 1 cubic millimeter. Specifically these materials consist of the hone, white matter, gray matter, fluid (cerebrospinal fluid/blood), and blood vessel

> The Sierra/SM finite element mesh of the test object consists of 12 million linear hexahedra, with a maximum element size of 0.5 cubic millimeters. The bone, white matter, gray matter CSF and vascular walls have been modeled with a conforming geometry

### **Computational Results**



### Conclusions

Computer simulations based upon material models matched to human tissue predict a predilection of cavitation and dilatational forces at the same interfaces found to have astroglial scaring in blast traumatic brain injury. Such findings require further experimental validation but may suggest cavitation and dilatation are mechanical forces important in causing brain tissue damage in blast traumatic brain injury

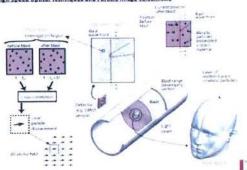
Laboratories

### **Experimental Validation**

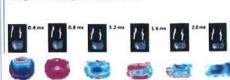
Brain Simulant - See poster MHSRS 17 1710 Materials Characterization of Cramial Smulants for Blast Induced Traumatic Brain Injury

Eabrication Techniques -- See poster MHSRS 17.3718 Additive Manufacturing of Cranial Simulants for Blast Induced Traumatic Brain Injury

High Speed Optical Techniques and Particle Image Velocimetry



Dynamic measurement with ultra high speed imaging while the blast wave is crossing the test object (above). Cavities in the test object have dimensions similar to those in the brain (zoomed in view, upper left corner). Metallic particles embedded in the test object will trace strain as the detonation wave propagates (zoomed in view at the edge of the detonation wave, above center) Particle image Velocimetry (P(V) [11] will be used to generate 20 vector fields representing strain and strain rate (schematic of PiV process on the right). Helow is the material velocity vectors of ballistics gel undergoing blunt trauma (hammer) far right is velocity magnitude of vectors in m/s.



### References

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